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Dated 10th December, 1993.

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30 MAR 1992

Official use

-2APR 1992H00308647

PAT 1 77 UC

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# Request for grant of a Patent

Form 1/77

Patents Act 1977

**① Title of invention**

Imaging Apparatus and Method

1 Please give the title  
of the invention

**② Applicant's details**☐ **First or only applicant**

2a If you are applying as a corporate body please give:

Corporate name

Country (and State  
of incorporation, if  
appropriate)

2b If you are applying as an individual or one of a partnership please give in full:

Surname	Filler
Forenames	Aaron Gershon

2c In all cases, please give the following details:

Address	31 Copse Hill
	Wimbledon

UK postcode (if applicable)	SW20 ONE
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Country	U.K.
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ADP number (if known)	5708722001 80
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**2d, 2e and 2f:** If there are further applicants please provide details on a separate sheet of paper.

☐ **Second applicant (if any)**

**2d** If you are applying as a corporate body please give:

Corporate name

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**2e** If you are applying as an individual or one of a partnership please give in full:

Surname Howe

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(if applicable)

SW17 ORE

Country

ADP number  
(if known)

U.K.

6081970001

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Form 51/77.  
1-12-93.

**③ Address for service details**

**3a** Have you appointed an agent to deal with your application?

Yes ☐

No ☒ → go to 3b

↓  
please give details below

Agent's name

Marks + Clerk

Agent's address

57-60 Lincoln's Inn Fields  
London

Postcode

WC2A 3LS.

Agent's ADP  
number

**3b:** If you have appointed an agent, all correspondence concerning your application will be sent to the agent's United Kingdom address.

**3b** If you have not appointed an agent please give a name and address in the United Kingdom to which all correspondence will be sent:

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Address

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ADP number  
(if known)

Daytime telephone  
number (if available)

(081)946-7711

**④ Reference number**

- 4 Agent's or applicant's reference number (if applicable)

**⑤ Claiming an earlier application date**

- 5 Are you claiming that this application be treated as having been filed on the date of filing of an earlier application?

Yes ☐ No ☒ ➔ go to 6

↓  
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- ☐ number of earlier application or patent number

- ☐ filing date (day month year)

- ☐ and the Section of the Patents Act 1977 under which you are claiming:

15(4) (Divisional) ☐ 8(3) ☐ 12(6) ☐ 37(4) ☐

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- 6 If you are declaring priority from previous application(s), please give:

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⑥ If you are declaring priority from a PCT Application please enter 'PCT' as the country and enter the country code (for example, GB) as part of the application number.

Please give the date in all number format, for example, 31/05/90 for 31 May 1990.

- 7 The answer must be 'No' if:
- any applicant is not an inventor
  - there is an inventor who is not an applicant, or
  - any applicant is a corporate body.

8 Please supply duplicates of claim(s), abstract, description and drawing(s).

Please mark correct box(es)

- 9 You or your appointed agent (see Rule 90 of the Patents Rules 1990) must sign this request.

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## 7 Inventorship

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No ☐

A Statement of Inventorship on Patents Form 7/77 will need to be filed (see Rule 15).

## 8 Checklist

8a Please fill in the number of sheets for each of the following types of document contained in this application.

Continuation sheets for this Patents Form 1/77

*J*

Claim(s)

3

Description

15

Abstract

1

Drawing(s)

4

8b Which of the following documents also accompanies the application?

Priority documents (please state how many)

Translation(s) of Priority documents (please state how many)

Patents Form 7/77 – Statement of Inventorship and Right to Grant (please state how many)

Patents Form 9/77 – Preliminary Examination/Search

Patents Form 10/77 – Request for Substantive Examination

## 9 Request

I/We request the grant of a patent on the basis of this application.

Signed

*Frulipe Kave*  
*Alan G. Hill*

Date 28 March 92  
(day month year)

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## IMAGING APPARATUS AND METHOD.

The present invention relates to an imaging method and an apparatus for performing same. In particular, it relates to a new method for making a type of image of the living mammalian body such as of a human. The resultant image is hereinafter referred to as a neurogram or image neurogram and which shows the pattern of the peripheral, autonomic or cranial nerve tree so that it stands out in isolation from other structures.

Although many techniques have been developed for showing distinctive images of the brain, spinal cord, and spinal roots within the spinal canal, hitherto there has not been a successful method for creating images of the peripheral, autonomic, and cranial nerves as they pass among bones, muscles, lymphatics, tendons, ligaments, intermuscular septa, collections of fatty tissues, air or fluid spaces, veins, arteries, joints, skin, mucous membranes and other tissues or of cancelling the image signal of these various non-neural tissues in order to appear to enhance the nerve in such a way as to permit neurographic images. The peripheral, autonomic, and cranial nerves are relatively small compared to many other bodily tissues, and they often travel in bundles near other structures of comparable size and shape.

The lack of a suitable method for creating a distinct image of the nerves in a living mammal or human has been a great hindrance to physicians, surgeons, athletic trainers, and pain treatment specialists. Such a neurogram would also be of great advantage to designers of ergonomic furniture, specialized body suits, boots, and various kinds of electronic or electric medical equipment which can be best used when the positions of nerves can be precisely located in advance.

Although many nerves travel along straight and simple courses, there are very complex nerve arrangements such as the brachial plexus, lumbar plexus, or sacral plexus where bundles of nerves collect together, separate, rejoin, intermix, and resegment in such a way as to create a very intricate three dimensional pattern. A compression or irritation of a small area of nerve within such a plexus (e.g. in the shoulder) can cause pain, numbness, weakness or paralysis at some distant site (e.g. in one finger). Even when a surgeon attempts to expose and examine the brachial plexus for direct inspection, the anatomic complexity can prove overwhelming, rendering surgery in this area to be extremely difficult and dangerous.



Unpublished co-pending PCT Patent Application No. PCT EP 91/01780 describes a method which attempts to make nerves stand out in images by the means of administering pharmaceutical agents which give the nerves special imaging properties. These pharmaceuticals are two-part agents which gain entry into and are transported within nerves where the second part of the agent has an imageable property.

If the second part of the molecule has elements with high nuclear density, then it may tend to increase the contrast of the nerve upon X-ray or Computed Tomography (CT) examination.

If the second part has a radioactive (e.g. positron emitting) element, then the nerve may be visible upon Positron Emission Tomography (PET) scanning, or if the second part has a magnetically active component, then the signal of the nerve may be changed upon Magnetic Resonance Imaging (MRI). These agents are injected into muscle and thereby used selectively to alter the imaging characteristics of the nerve supplying that muscle.

The main limitation with these intraneural pharmaceutical agents is that they can generally be used only to image a single nerve or nerve group. The MRI agents for nerve imaging actually gain their effect by blacking out the nerve in the image. Since nerves are difficult to see in current types of MRI images, the action of these MRI nerve imaging agents can be difficult to interpret.

The present disclosure relates to a new method, which quite remarkably, is capable of generating a three dimensional image of an individual patient's nerves and nerve plexuses. The image can be acquired non-invasively and rapidly by a magnetic resonance scanner. These images are acquired in such a way that some embodiments of the invention are able to make all other structures in the body including bone, fat, skin, muscle, blood, and connective tissues seem to tend to disappear so that only the nerve tree remains to be seen. A plurality of the nerves passing through a given imaged region may be observed simultaneously thus alleviating any ambiguity of nerve identification which might arise were only a single nerve imaged as with some contrast agent techniques.

Thus, a first aspect of the present invention provides a method of selectively imaging neural tissue of a subject without requiring use of intraneural contrast agents, the method comprising subjecting part of the subject anatomy to magnetic resonance

imaging fields, detecting magnetic resonance and producing an image of neural tissue from said electronic signal so that in said image, a nerve, root or neural tract of interest can be visually differentiated from surrounding structures.

It is important to realise that although previously, it has sometimes been possible to make a nerve stand out from immediately surrounding structures, it is the unique, very useful, and novel ability to make the nerve stand out from all other structures which is a significant advantage of the present invention. This is an important distinction in the area of 3-dimensional reconstruction since the use of gray-level gradient shading and surface rendering is difficult when applied to very small structures such as some nerves. By reducing all other structures below the intensity of nerve as described hereinbelow, it becomes possible to employ, among other techniques, simple threshold algorithms and, importantly, maximum intensity projection to achieve good quality 3D rendering for structures close in size to a single image voxel in the course of applying ray casting or other 2D or 3D projection methods.

Where all non-nerve tissue can be reduced to relatively very low intensity, or indeed be caused to disappear entirely from the image it becomes readily possible to program a computer to identify the nerve locations in the anatomical structure and to correctly trace the course of the nerves between 2D image planes or through a 3D acquisition volume. The ability to correctly trace the course of a nerve through its anatomical relations and over the course of its various divisions and ramifications is a significant aspect of the invention. This is because a 2D image may demonstrate various bright dots representing the cross section of nerves. However, with other anatomical information deleted, it is often important to be able to reconstruct the nerve tree in order to correctly identify precisely which nerve is which in any given 2D section, 2D projection, 3D projection, rendering or perspective display, whether or not that display is susceptible to rotation on the computer screen to aid the user of the image.

Preferably, the image selectivity for nerves is provided by discriminating properties of water diffusion anisotropy or of proton fast exchange rates or of  $T_1$  but optimally  $T_2$  relaxation rates as will be described in more detail hereinbelow.

A second aspect of the present invention provides a method of selectively imaging neural tissue of a subject, the method comprising subjecting part of the subject anatomy to magnetic resonance imaging fields adapted to discriminate anisotropy of water diffusion or other special characteristic of neural tissue, detecting magnetic



resonance to produce an electronic signal in accordance with said resonance and producing an image of neural tissue from said electronic signals.

Preferably, the imaged neural tissue constitutes the main, or even the only, structure visible. The imaged neural tissue may be selected and physically aligned tracts of neural tissue.

Neurographic imaging effected in accordance with the present invention utilises a set of special pulse sequence and program instructions to control the electronic equipment of an MRI scanner. For the imaging of fine nerve branches, the pulse sequences can be aided by the use of special signal and imaging coils placed near or around the portion of the body of greatest interest. This does not require the administration of any pharmaceutical agent. Indeed, since neurographic imaging makes nerves appear bright and isolated in an image, it then becomes far more informative to selectively black out one of the nerves by means of administering an intraneural pharmaceutical contrast agent.

Thus image neurography can be viewed as a way of effecting a process which rapidly produces an image of an entirely new kind, wherein that image can be examined for its anatomical information content, and wherein that image can be manipulated by the administration of pharmaceutical agents such as intraneural contrast agents or intravenously administered contrast agents or other types of contrast agents which have effects upon magnetic resonance signals.

The aforementioned intraneural nerve imaging pharmaceutical agents were designed to help in the diagnosis of nerve compressions and nerve compressions and nerve injuries, it was not anticipated that the nerves could be seen in relative isolation without administering any pharmaceutical. Indeed, users of such agents have acutely appreciated the need for some imaging technique which would synergistically render the effects of the intraneural agents into much more useful form, although neurography per se had not been appreciated as the solution to this problem, nor had any proposal to attempt to accomplish branching image neurography been made.

The fine spatial resolution required for creating detailed images of peripheral nerves, including their small distal ramifications and divisions, is well within the physical range of current clinical magnetic resonance imaging instruments, particularly when specially designed local signal and imaging coils are used.

The inventors have discovered that there are various different sets of pulse sequences and combinations of pulse sequences which can be used to unambiguously distinguish small nerves from neighbouring structures of similar shape and location. This includes the combination of some existing sequences into new groupings for use in new situations as well as the design of new sequences which incorporate optimized features for the purpose of neurographic imaging.

The ideal 'neurographic image' is analogous to a subtraction angiogram (an image showing only blood vessels), but sharply highlights a nerve rather than a vessel. Such an image is most useful for confirming the identification of nerves in a given imaging plane or space as well as for locating nerve injuries and nerve compressions. Despite the well known existence of angiograms showing the entire vascular pattern in an anatomic regions, and despite the existence for many years of various magnetic resonance techniques which could have been applied to the creation of neurograms, and despite the lack of any feasible method for visualizing nerves in isolation, there has not previously been any way of creating neurograms.

An important obstacle to the invention of neurograms has been the difficulty of knowing with assurance that a given structure in an image plane actually is a nerve as opposed to some other structure similar in shape and location. The inventors have solved this problem by discovering a set of pulse sequences which can unambiguously prove that a given structure in an image is indeed a nerve. Using this tool, it was then possible to discover other simpler pulse sequences which achieved the same image result when applied to the same subject in the same scanner during an imaging session. In this fashion, by first confirming the nerve images, and by then using the firm data to cross check the results of other techniques useful for various reasons, it was possible to build up a collection of techniques capable of application for practicing the invention, e.g. for producing image neurograms with a magnetic resonance scanner.

The inventors have carried out experiments in which they tested imaging techniques which enabled them to selectively delete the signal from non-neural structures and also evaluated techniques which permitted relative enhancement of the image signal from nerve. One discovery was that neurographic imaging could be greatly aided by taking special advantage of the "anisotropic water diffusion" which is known to take place in muscle, in the central nervous system and in peripheral nerves. Stated simply, water diffusion occurs preferentially along the axial length of nerves, more than radially across the nerve tissue. This directional preference for diffusion may be detected by magnetic resonance imaging, more especially by proton nmr

imaging. However, nmr utilising other magnetic resonance susceptible nuclei may also be used, e.g.  $^{19}\text{F}$ fluorine,  $^{13}\text{C}$ carbon,  $^{31}\text{P}$ phosphorus, deuterium or  $^{23}\text{Na}$ sodium.

For a preliminary enhancement of the image of the nerves, it is preferable to apply a process to eliminate non-neural signals during the magnetic resonance imaging, for example by suppression of resonance signals from fat. Fat suppression may for example be effected by chemical shift selection or by selective water stimulation. Other means to achieve fat suppression include the Dixon technique and also STIR (short tau inversion recovery) which can be used for neurography.

The inventors have demonstrated that, under ideal image collection and pulse sequence circumstances, the diffusion coefficient of anisotropy in peripheral nerve is greater than that in muscle, and that it was possible to collect appropriate diffusion weighted images after preliminary fat suppression in such a way as to generate image neurograms or to reliably identify nerves.

In the imaging method according to the present invention, it is preferred that magnetic diffusion weighted field gradients are applied in at least two different directions and the signals from the respective resultant resonances are subtracted to produce said discrimination of water diffusion anisotropy. Most preferably, the magnetic field gradients are applied in mutually substantially orthogonal directions.

It is also possible in many anatomical regions to achieve adequate enhanced isolation of the nerve image by applying only a single diffusion gradient perpendicular to the long axis of the nerve at the site of interest. When this is adequate, then no subtraction need be carried out to produce the neurogram. The fat suppressed orthogonally diffusion weighted image can either be processed directly, or it can be subject to threshold processing which will remove signals of lower intensity from non-neural tissue or from nerves with different long axis and direction of travel at the imaging location.

Similarly, in some regions of interest, it is possible to achieve adequate enhanced isolation of the nerve image by use of a spin echo fat suppression technique with a long TE (echo time) between 50 and 100 milliseconds. This is because after fat suppression, the dominant signal to suppress is from muscle. Since the  $T_2$  of muscle is approximately 27 milliseconds while the  $T_2$  of peripheral nerve is approximately 55 milliseconds (both as measured by the inventors) there is a factor of two difference between the two types of tissue. The inventors have used this technique

to produce images in which nerves are brighter than any other structure in the image and which images are therefore susceptible for use in constructing neurograms.

Yet another means of accomplishing the secondary nerve enhancement is by means of a magnetisation transfer pulse sequence after the fat suppression. Because of the relatively slow rate of exchange between the off-resonance relatively stationary protons in myelin sheath and the on-resonance mobile protons of axoplasmic water, there is a differential sensitivity between nerve and muscle when magnetisation transfer is applied.

Still another means of practicing neurography is by optimizing sequences to be sensitive to the slow coherent flow of the endoneurial fluid. This provides a unique signal because of its proximal to distal direction of flow and because of its slow rate which can be monitored by techniques originally developed to distinguish diffusion from perfusion, including velocity compensation by first order gradient nulling as well as others, which detect flow and can be optimized for very slow directional flow rates.

The present invention also includes a method of diagnosis or physiological investigation comprising application to a part of the subject anatomy of an imaging method according to the present invention as hereinbefore described.

Various diagnostic applications of the method of the present invention may be better understood with reference to Figure 1 of the accompanying drawings, which shows a sectional view through a vertebra. The structures and conditions illustrated are denoted by the following reference numerals:-

- |                        |  |
|------------------------|--|
| 9. Herniated Disc      |  |
| 10. Compressed Root    | 18. Dorsal Ramus                             |
| 11. Spinous Process    | 19. Dorsal Root Ganglion                     |
| 12. Anulus Fibrosus    | 20. Facet                                    |
| 13. Nucleus Pulposus   | 21. Dorsal Root                              |
| 14. Autonomic Ganglion | 22. Extradural Fat                           |
| 15. Ventral Root       | 23. Root in Cauda Equina                     |
| 16. Ventral Ramus      | 24. Dural Sac                                |
| 17. Transverse Process | 25. Cerebrospinal Fluid within<br>Dural Sac. |

In this diagram, the two features of interest are the left spinal root (10) and the left ventral root which are both in risk of compression from the herniating disc (9). Both nerves are travelling through fat (22) but are surrounded by bone (which could impair observation by an X-ray based technique) and are near the strong water signal of disc and of cerebrospinal fluid in the dural sac (25) and other inflamed tissue (which often diminishes image resolution and quality in generally used magnetic resonance techniques).

The structures of diagnostic interest (10 and 15) are small relative to the large number of other anatomic structures nearby. Also note that (10) and (15) are nearly perpendicular to each other. This very common imaging problem could now be approached by applying fat suppression, then selecting orientations for pulsed diffusion gradients which enhanced either the spinal root (10) or the ventral root (15) so that each could be clearly seen in a given image and carefully examined for evidence of compression or inflammation.

Other diagnostic applications include the following:-

1. Demonstrating the anatomy of peripheral, cranial, and autonomic nerves and nerve plexuses.
2. Demonstrating the anatomy of spinal roots, particularly, cervical, thoracic or lumbar spinal roots where they pass through fat at the foramina through which they exit the spinal canal.
3. Demonstrating the anatomy of spinal roots within the lumbar canal where they pass through quantities of extradural fat.
4. Examining cranial nerves for compressions by vessels or other structures which could cause trigeminal neuralgia (Vth nerve), hemifacial spasm or Bell's palsy (VIIth nerve), essential hypertension (Xth nerve) or other cranial nerve syndromes.
5. Demonstrating nerve, plexus or root compressions or injuries where abnormal changes in the direction, position, or other diffusional properties are caused by an injurious process, such as nerve transection, demyelinating diseases, peripheral neuropathies and crush injuries. These concerns apply similarly to monitoring the regrowth of nerves.

6. Exploring the location of tumours or other masses within the spinal cord where it is useful to know the position of cortico-spinal motor tracts or other functional white matter long tracts relative to some abnormality.
7. Demonstrating the anatomy of the optic nerve, an extension of the brain, where it passes through the peri-orbital fat other fat on its route to the retina.
8. Tract tracing within the brain in order to provide useful images for study by radiologists, surgeons or physicians. In particular, for identification of the location of areas of 'eloquent cortex' such as the motor strip, or speech related areas. This method involves the spatial identification of relevant areas of the thalamus and then following projecting tracts to the area of interest on the cortical surface, or identify regions of interest by reference to their connections with other areas on the cortical surface.
9. Tracing of nerves as they pass through tumours of low diffusional anisotropy. Such as the passage of the VIIIth nerve through an acoustic neuroma in order to permit a surgeon to know the location of the nerve in or near the tumour and so to have the ability to avoid the nerve during surgery on the tumour.
10. Application of diffusion anisotropy imaging for the evaluation of diffuse axonal injury, as may occur in head injury.

The first aspect of the invention also provides an apparatus for selectively imaging neural tissue of a subject without requiring the use of neural contrast agents, the apparatus comprising means for subjecting part of the subject anatomy to magnetic resonance fields, means for detecting magnetic resonance to produce an electronic signal in accordance with said resonance and means for producing an image of neural tissue from said electronic signal so that in said image, a nerve root or neural tract of interest can be visually differentiated from surrounding structures.

The second aspect of the present invention also finds expression as an apparatus for imaging neural tissue of a subject, the apparatus comprising means for subjecting part of the subject anatomy to magnetic resonance fields adapted to discriminate anisotropy of water diffusion, means for detecting magnetic resonance to

produce an electronic signal in accordance with said resonance and means for producing a selective image of neural tissue of interest from said electronic signal.

Preferably, any apparatus according to the invention also comprises a coil for application of a radiofrequency field to said anatomy part and/or for detection of a resonance signal, wherein said coil is configured and dimensioned to fit closely over said anatomical part.

Conveniently, the coil is a solenoid coil or surface coil and is configured and dimensioned to fit closely over a human limb, shoulder, chest, pelvic region, head, neck or back.

In principle, selective imaging of part of any other object or subject may be effected using magnetic resonance if that subject or object exhibits diffusion anisotropy in any part thereof. Thus, in medicine, for example a part of the cardiovascular system could be imaged in similar fashion. However, the technique could also be applied to rock strata, plants etc if diffusion anisotropy occurs in same.

Thus a third aspect of the present invention provides a method of selective imaging, the method comprising observing diffusion anisotropy.

The third aspect of the invention also provides a magnetic resonance apparatus for selective imaging, said apparatus being adapted to discriminate diffusion anisotropy.

The present invention will now be explained in more detail by the following description of a preferred embodiment and with reference to the accompanying drawings, in which:-

Figure 1 shows a section through the lumbar spinal canal and a lumbar vertebra with a herniated disc to indicate the size and location of the nerves and their surrounding structures ;

Figure 2 shows a magnetic resonance imaging apparatus for use in accordance with the present invention;

Figure 3 shows an example of pulse sequencing for operating the apparatus shown in Figure 1;

Figure 4 shows a diagram of a transverse section of the upper fore-arm of a rabbit based on the fat suppressed image shown in Figure 5. 201) triceps muscle, 202) ulnar nerve, 203) brachial veins, 204) median nerve, 205) radial nerve, 206) humerus, 207) cephalic vein, 208) biceps muscle;

Figure 5 shows a fat suppressed image in which black represents highest intensity of resonance signal;

Figure 6 shows the effect of application of a perpendicular pulsed gradient renders the nerves as the highest intensity features in the image; and

Figure 7 shows the effect whereby reorienting the gradient parallel to the long axis of the nerve has a relatively greater effect in reducing the nerve signal than that of the muscle.

Figure 2 shows an example magnetic resonance imaging apparatus 101 suitable for use in the present invention. It comprises a magnet 103 and a tuned radiofrequency (rf) coil 105 for excitation of the nucleus and detection of the required signal (separate transmit and receive coils may also be used). This coil is placed over a limb 107 under investigation.

One pair of a set 109, 111 of three pairs of coils used to generate a magnetic field gradient over the sample region. A computer 113 is used to control and synchronise the necessary electronic devices of the MRI and process to display the acquired data. An interface bus 115 is arranged between the computer and the electronic devices. A device 117 is used to generate the required radiofrequency pulse shapes. Another device 119 is used to generate the required gradient pulse shapes.

The device 117 is connected to a high power radiofrequency amplifier 121 for the rf pulses. Another amplifier 123 (one of three) is connected to the device 119 and has an output arranged to drive the gradient coils.

A duplexer 125 is arranged to steer the high power rf pulses from amplifier 121 to the coil 105 and steer the very low signals received by the coil to a preamplifier 127 for the received NMR signals. A mixer 129 is connected to the preamplifier to transform the high frequency nmr signals to low frequency signals by mixing with



signals from a digitally controlled rf oscillator 131. The output of the mixer is connected to an analogue-to-digital converter 133 via a low pass filter 135.

Operation of the apparatus shown in Figure 2 to perform an imaging method according to the present invention may be understood better from the pulse sequences illustrated, by way of example only, in Figure 3.

Frequency selective pulses A,B and C selectively excite the nuclear spins of the fat molecules and the gradient pulses a, b, and c (along axes X,Y and Z respectively) dephase these spins thereby minimising the contribution of the fat signals to the final image. This is the known fat suppression technique using CHESS (Chemical Shift Selective) pulses.

A spin echo signal F, is generated by the combination of the radio-frequency excitation pulse D and refocussing pulse E. The pulsed gradients d to g are the imaging gradients used to encode the signal F in the usual manner such that an MRI image may be constructed. The sequence may be used to generate images from contiguous slices of the sample/patient under investigation.

The echo signal F, and therefore the pixel intensity in the constructed image is made sensitive to the spatial diffusion of the water molecules by the addition of the pulsed gradients h and h' known as the "diffusion sensitizing gradients". Spatial anisotropy in the molecular diffusion is determined by comparing two or more images acquired with the diffusion sensitizing gradients oriented along different axes. The images are obtained in such a way to minimise motion artefacts by acquiring the data for the different diffusion sensitizing gradients in an interleaved manner.

In the case of a major axis of known diffusion anisotropy (e.g. a nerve tract) a simple 'image neurogram' may be generated by simply subtracting the appropriately scaled image obtained with the diffusion sensitizing gradient oriented parallel to the nerve tracts from a scaled image obtained with the diffusion sensitizing gradient oriented perpendicular to the nerve tracts.

If the major axis of diffusional anisotropy is not known, a plurality of images are acquired with different orientations of the diffusion sensitizing gradients. The image data can then be processed to give a parameter associated with each pixel (or voxel in a 3D data set) which is a measure of the diffusional anisotropy at that point reflecting both magnitude and direction.

The method used in this embodiment first carries out the fat suppression technique which maintains excellent image resolution, or uses a sequence which selectively excites only the water signal so that fat does not contribute to the final image and then, within the same pulse sequence, optionally includes an oriented pulsed gradient for selective incorporation of information from diffusion anisotropy.

The various parts of the pulse sequence are selected so as to optimally destroy as many other signals as possible other than that of nerve as shown in Figure 7. Then, optionally, a second sequence is carried out which selectively destroys the nerve signal as by for instance, rotating the diffusion gradient orientation to be parallel rather than perpendicular to the nerve as shown in Figure 8.

The effect of these manoeuvres is to produce two images, the first of which shows up the nerve relatively brightly, and the second of which selectively destroys the nerve signal. When these two penultimate images are then mathematically or photographically, or optically subtracted from one another, and optionally divided by the signal information from a fat suppressed T2 weighted spin echo sequence (e.g. using the aforementioned CHESS technique), the result is the neurogram.

An alternative approach would be to use pulsed gradients oriented in each of a plurality of or into specially created axes suitable to the imaging task. In this fashion, it is possible to determine a parameter which characterised the diffusion coefficient anisotropy for each voxel in the image, including both magnitude and direction. This parameter can be rendered to produce a neurographic image for good image registration.

To optimize the technique where data processing requires the manipulation of the image data on a point by point basis between a plurality of image data sets, the image sequence can be modified to interleave the different sequences and so to minimise any motion artefact which could degrade the accuracy of the final image when the different sequences are collected at times separated by several minutes. Furthermore the image sequence can be synchronised to respiration or to the heartbeat to additionally reduce the effects of motion. It is also possible to carry out the signal acquisition using a so called "three dimensional" imaging sequences processed by using a 3D Fourier transform.

Images were obtained with a 4.7 Tesla, 33cm bore SISCO system fitted with a 10 Gauss/cm high performance auxiliary gradient insert (12 cm inner bore). A three-turn solenoid coil (2.5 cm in length and 3cm in diameter) was placed around the upper portion of the forelimb of 2 - 2.5 kg rabbits. The animals were maintained under balanced continuous intravenous infusion of an anaesthetic mixture containing 1 mg of medazolam, 1.5 mg of fluanisone and 50  $\mu$ g of fentanyl per ml at rates of 4 to 10 ml/hr to achieve a deep anaesthesia minimising motion artefacts from respiration.

A specially modified multislice spin echo imaging sequence (TE=40 ms, TR=1 sec) was adjusted to provide fat suppression (CHESS) and to accommodate diffusion weighting of images. This set of modifications allows operator control of the strength of the gradients and allows various strengths and orientations to be inserted into 'slots' or reserved times within the common base sequence. After an initial image with fat suppression only, there is next collected one image with diffusion gradients perpendicular to the image plane and then one image with diffusion gradients parallel to the image plane.

The CHESS sequence consisted of a 3 millisecond (ms) gaussian pulse for selective excitation of fat followed by a 5 Gauss/cm dephasing gradient of 3 ms duration performed 3 times with orthogonal gradients prior to each spin echo sequence. For diffusion weighting, pulsed gradients of strength  $G_i=10$  G/cm, duration  $\delta=7$  ms, and separation  $\Delta=20$  ms, were symmetrically placed about the  $180^\circ$  pulse. Transverse images (nerves primarily orthogonal to image plane) with slice thickness of 2 mm were obtained for a 4 cm field of view with 256 phase encoding steps. Image data was zero filled to 512 points to give 78 $\mu$ m in plane resolution.

Simple spin echo images of limb anatomy proved inadequate for definitive identification of peripheral nerves because the nerves are typically surrounded by the high intensity signal from fat deposits in the intermuscular spaces. Further, there are a variety of structures similar to nerve in size and shape which follow similar routes.

However, it was found that the fat surrounding nerves is actually beneficial for nerve identification, because in a fat suppressed image, a relatively high intensity nerve signal stands out sharply within the very low intensity space left behind by the suppressed fat signal as shown in Figure 5.

Under these conditions the phenomenon of diffusion anisotropy was applied to the problem of nerve image enhancement and shown to be exceedingly effective (see

Figure 4 to 7). Apparent diffusion coefficients perpendicular and parallel ( $D_{\perp}$ ,  $D_{\parallel}$ ) were calculated from average pixel intensity measurements over the region of interest (ROI) from each of the three different images in a given set. Calculation employed the formula ( $\text{Intensity} = A_0 \cdot \exp[-TE/T_2] \cdot \exp[-bD]$ , attenuation factor  $b = \gamma^2 G^2 \Delta^2 [\Delta - \partial/3] = 61.9 \cdot 10^3 \text{ sec/cm}^2$ ).

Apparent Diffusion Coefficients ( $10^{-5} \text{ cm}^2/\text{sec}$ )

	Muscle	Median Nerve
$D_{\perp}$	1.2	0.98
$D_{\parallel}$	1.8	2.3
$D_{\parallel}/D_{\perp}$	1.5	2.35

This example demonstrates that fat suppression by CHESS enhances the visualization of peripheral nerves so that when different diffusion gradient orientations are incorporated in secondary segments of the imaging pulse sequence, the ultimate yield is a far larger relative change in intensity in the nerve signal than in muscle.

This intensity change then provides the basis for an image subtraction technique to achieve relative nerve image enhancement. The various subtracted or divided nerve images are then assembled mathematically by routine reconstruction techniques into a three dimensional image. Thus the objective of assembling three dimensional neurograms is conveniently achieved.

In the light of this disclosure, modifications of the described embodiment, as well as other embodiments, all within the scope of the present invention as defined by the appended claims, will now be apparent to persons skilled in the art.

## CLAIMS

1. A method of selectively imaging neural tissue of a subject without use of neural contrast agents, the method comprising subjecting part of the subject anatomy to magnetic resonance imaging fields, detecting magnetic resonance to produce an electronic signal in accordance with said resonance and producing an image of neural tissue from said electronic signal so that in said image, a nerve or root or neural tract of interest can be visually differentiated from surrounding structures.

2. A method of selectively imaging neural tissue of a subject, the method comprising subjecting part of the subject anatomy to magnetic resonance imaging fields adapted to discriminate anisotropy of water diffusion, detecting magnetic resonance to produce an electronic signal in accordance with said resonance and producing an image of neural tissue from said electronic signal.

3. A method according to claim 2, wherein magnetic diffusion weighted field gradients are applied in at least two different directions and the signals from the respective resultant resonances are subtracted to produce said discrimination of water diffusion anisotropy.

4. A method according to claim 3, wherein said magnetic field gradients are applied in mutually substantially orthogonal directions.

5. A method according to any of claims 2-4, wherein a process to eliminate non-neural signals is applied during magnetic resonance imaging.

6. A method according to claim 5, wherein the process comprises suppression of resonance signals from fat.

7. A method according to claim 6, wherein said suppression is effected by chemical shift suppression.

8. A method according to claim 6, wherein said suppression is effected by selective water stimulation.

9. A method according to claim 5, wherein the process comprises magnetisation transfer.

10. A method according to any of claims 2-9, which method utilises proton magnetic resonance.

11. A method according to any of claims 2-10, wherein the image is a three dimensional image.

12. A method of diagnosis or physiological investigation comprising application to a subject of a method according to any preceding claim.

13. A method of selective imaging, the method comprising observing diffusion anisotropy by magnetic resonance.

14. An apparatus for imaging neural tissue of a subject, the apparatus comprising means for subjecting part of the subject anatomy to magnetic resonance fields adapted to discriminate anisotropy of water diffusion, means for detecting magnetic resonance to produce an electronic signal in accordance with said resonance and means for producing an image of neural tissue from said electronic signal.

15. An apparatus according to claim 14, further comprising a coil for application of a radiofrequency field to said anatomical part and/or for detection of a resonance signal, wherein said coil is configured and dimensioned to fit closely over said anatomy part.

16. An apparatus according to claim 15, wherein said coil is a solenoid coil or surface coil and is configured and dimensioned to fit closely over a human limb, shoulder, chest, pelvic region, head, neck, or back.

17. An apparatus for selectively imaging neural tissue of a subject without use of neural contrast agents, the apparatus comprising means for subjecting part of the subject anatomy to magnetic resonance fields, means for detecting magnetic resonance to produce an electronic signal in accordance with said resonance and means for producing an image of neural tissue from said electronic signal so that in said image, a nerve or root or neural tract of interest can be visually differentiated from surrounding structures.

18. A magnetic resonance apparatus for selective imaging, the apparatus being adapted to discriminate diffusion anisotropy.

19. A method of imaging neural tissue, the method being substantially as hereinbefore described with reference to any one of the accompanying drawings.

20. An apparatus for imaging neural tissue, the apparatus being substantially as hereinbefore described with reference to any one of the accompanying drawings.

ABSTRACT

IMAGING APPARATUS AND METHOD

In an apparatus and method for imaging neural tissue, a part of anatomy of a subject is subjected to magnetic resonance imaging fields. The fields are adapted to discriminate water diffusion anisotropy. Resonance signals are processed to produce the required image.



Fig 1

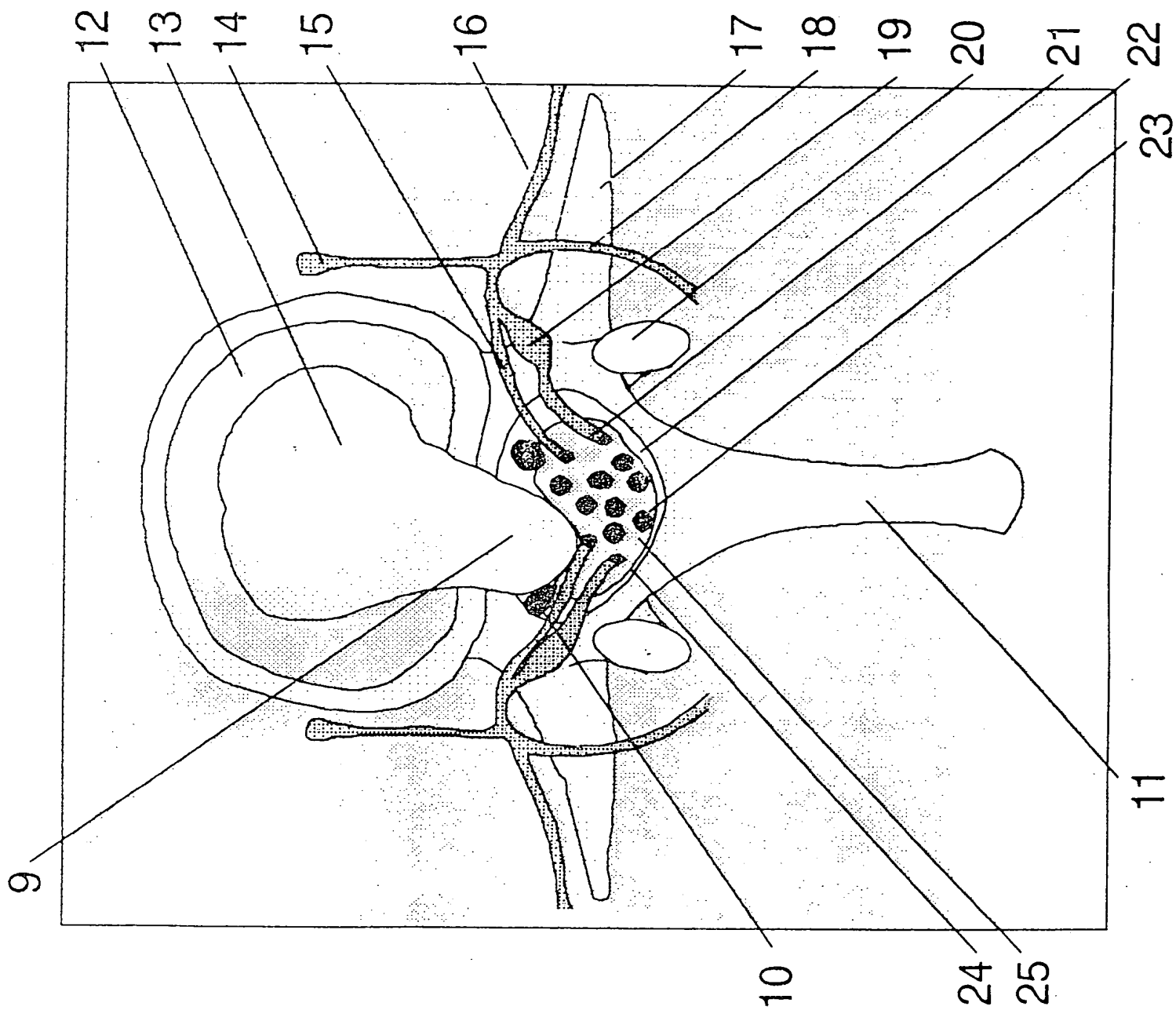
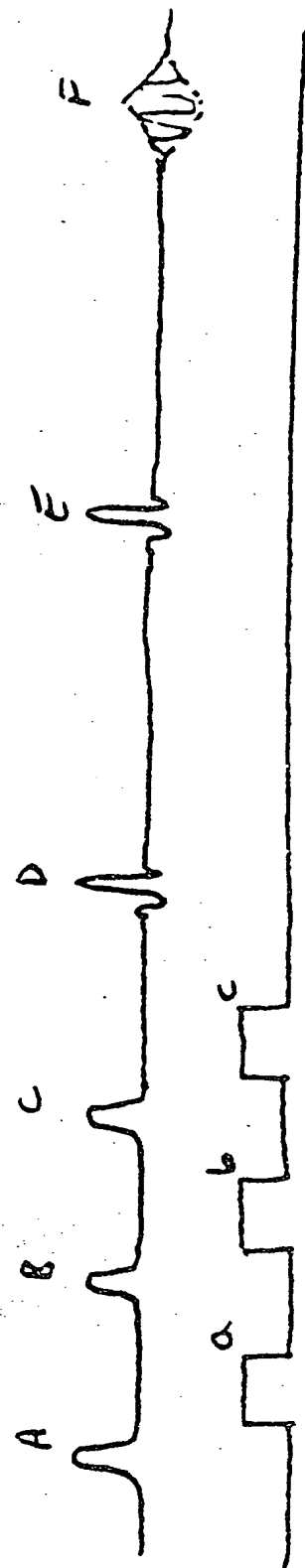




FIG 3

RADIOFREQUENCY  
PULSES



SPOILER  
GRADIENTS



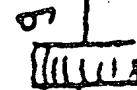
Slice selection  
GRADIENTS



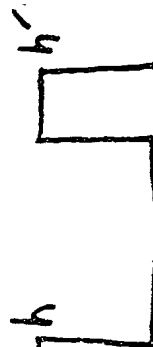
FREQUENCY  
ENCODING



PHASE  
ENCODING



DIFFUSION  
SENSITIVING  
GRADIENTS



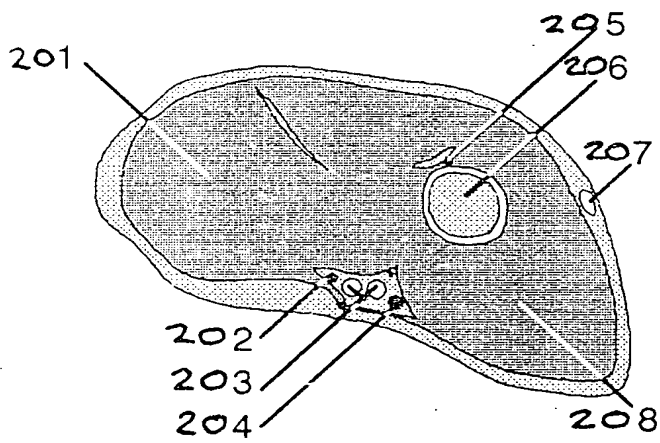


Figure 4

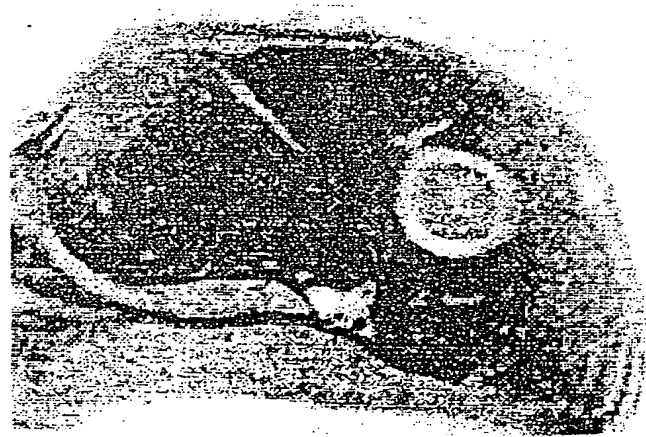


Figure 5

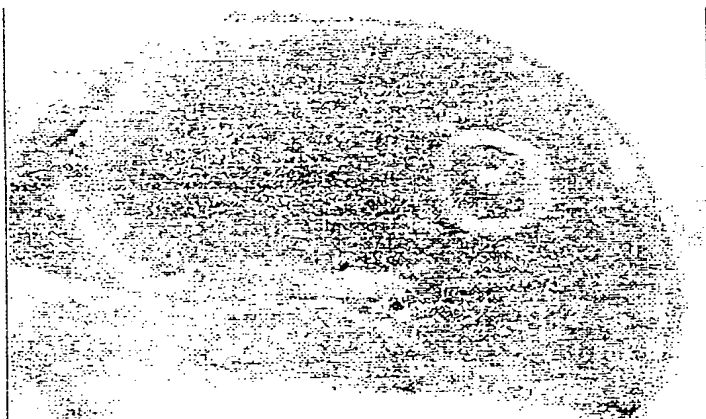


Figure 6

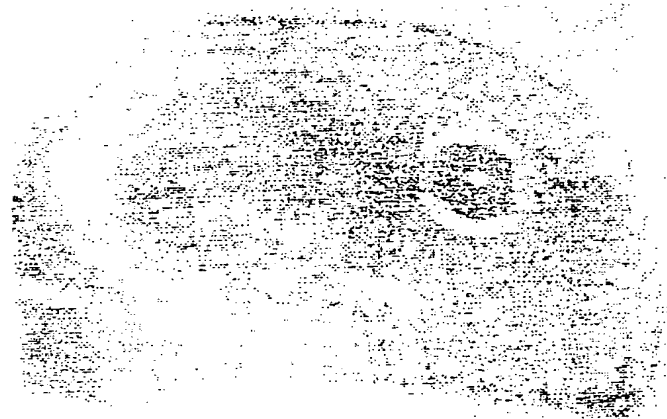


Figure 7